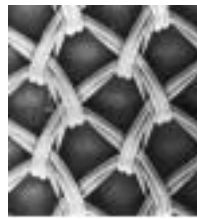
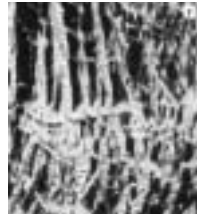


Based on their *pore size*, meshes can be classified into 4 types

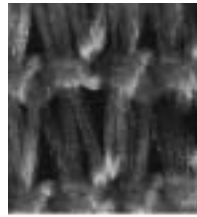
(Classification of Biomaterials, Amid 1997)¹



Type I Totally macroporous prostheses
(pores $>75\mu$)



Type II Totally microporous prostheses
(pores $<10\mu$)



Type III Macroporous prostheses with multifilamentous
or microporous components

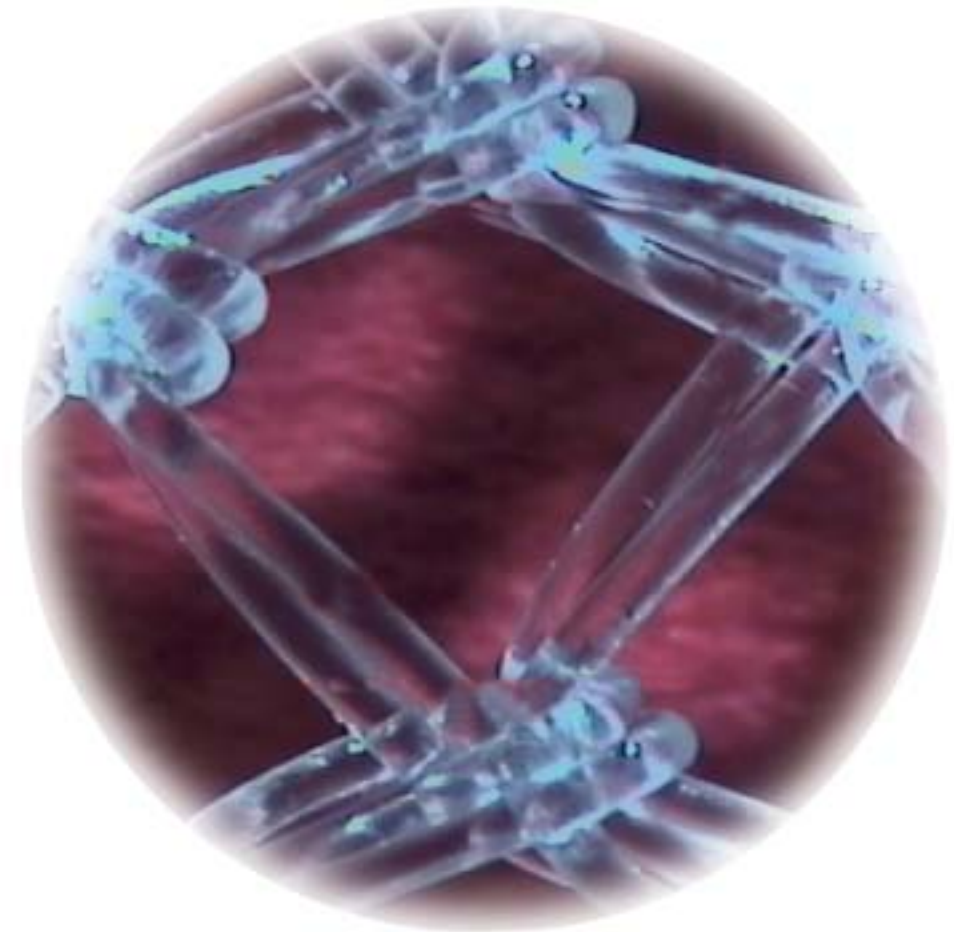


Type IV Submicronic pore size
(not a suitable prosthesis)

Type I meshes are preferable over all other types of meshes

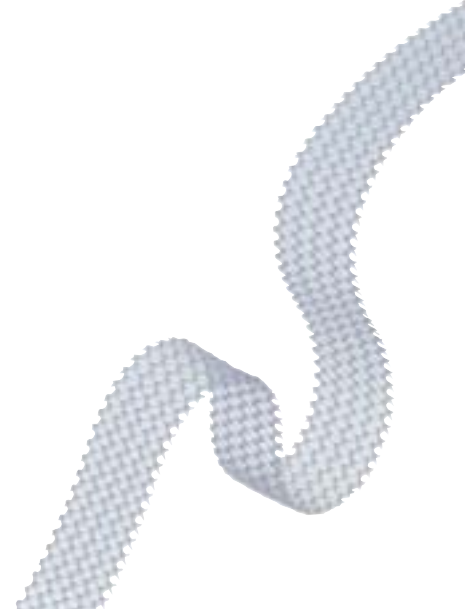
Advantages of Type I vs. Type II & III & IV: ¹⁻³

- Less foreign body reaction
- Less infection risk
- Rapid fibrinous fixation
- Greater tissue ingrowth

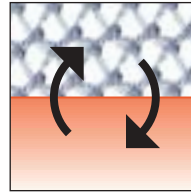


Selecting the Right Mesh

Important properties *of implant materials*
used in
**urogynecological
surgery**

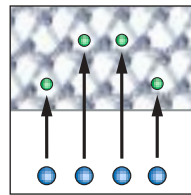


The most important *mesh properties:*



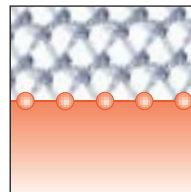
Inertness

- Meshes should be non-absorbable and permanent^{2,3}
- Polypropylene is the least reactive of all plastic materials¹⁻³



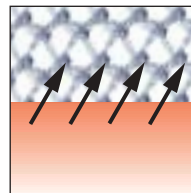
Resistance to infection

- Pores or interstices <10 μ prevent entry of macrophages and neutrophils, whereas bacteria which average only 1 μ can hide and proliferate in the mesh^{1-3,10}
- Macroporous biomaterials with pore size larger than 75 μ do not promote or harbor infection^{1-3,9}
- Totally macroporous meshes have the least risk of chronic infection¹⁻³



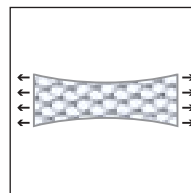
Rapid fibrinous fixation

- The ability of rapid fibrinous fixation is the function of sufficient molecular permeability of macroporous biomaterials^{1,2}
- This decreases the chance of seroma collection of potential dead spaces between the mesh and the host tissue. It results in formation of proper scaffolding for the future fibrocytic infiltration into the mesh^{1,2}
- Risk of seroma formation is virtually avoided by using macroporous prostheses¹



Host tissue incorporation

- Proper incorporation of fibroblasts, collagen and blood vessels require pore size >75 μ ^{1,2} (macroporous mesh, Type I)
- Slight roughness of the surface stimulates fibroplasia²
- Strength of attachment increases with pore size⁵



Elasticity

- Polypropylene meshes have a high tensile and bursting strength (resistance to breakage)⁴
- The elastic limit of the materials is unlikely to be clinically relevant as the forces exerted by intra-abdominal pressure increases are thought not to exceed 10-16 N⁶
- Macroporous polypropylene materials have the lowest initial stiffness i.e. the lowest resistance to deformation at forces below the elastic limit⁷

...and how the TVT Prolene™ Mesh *fulfills those properties:*

Inertness

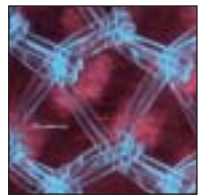
- Due to its unique chemical properties as a non-absorbable and permanent polypropylene suture, TVT Prolene™ causes a very limited foreign body



G. Beets⁸

Resistance to infection

- The macroporous, monofilament TVT (Type I) mesh allows macrophages entry into its pores and thus do not promote or harbor infection^{1-3,9,10}



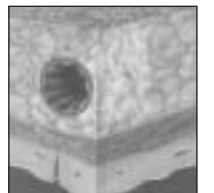
Rapid fibrinous fixation

- Due to its macroporous configuration, TVT minimizes the risk of seroma formation and allows the formation of a proper scaffolding^{1,2}



Host tissue incorporation

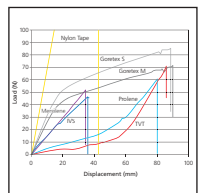
- TVT's uniform Interlock® structure with a pore size of 164 x 96 μ (Type I mesh) offers an excellent incorporation of the surrounding tissue during the healing process^{1-5,7}



G. Flesh¹¹

Elasticity

- Of all tested materials, TVT has the lowest resistance to deformation. TVT and other wide-weave Prolene tapes have unique biomechanical characteristics that may be at least partly responsible for the apparent clinical success of the implants and the very low erosion rates



H.-P. Dietz⁷

REFERENCES:

1. Amid P.K. Classification of biomaterials and their related complications in abdominal wall hernia surgery (Hernia 1997, 1:15-21)
2. Amid P.K et al. Biomaterials for «tension-free» hernioplasties and principles of their applications (Minerva Chir 1995 Sep, 50(9):821-6)
3. Goldstein H.S. Selecting the right mesh (Hernia 1999, 3:23-26)
4. Brenner J. et al. Mesh materials in hernia repair (Expert Meeting, Karger 1995, 172-9)
5. Bobyn J.D. et al. Effects of pore size on the peel strength of attachment of fibrous tissue to porous-surfaced implants (J Biomed Mater Res 1982 Sep, 16(5):571-84)
6. Schumpelick V. et al. Meshes within the abdominal wall (Chirurg 1999, 70:876-87)

7. Dietz H.P. et al. Mechanical properties of urogynecologic implant materials (Int Urogynecol J 2003, 14:239-243)
8. Beets G.L. et al. Foreign body reactions to monofilament and braided polypropylene mesh used as preperitoneal implants in pigs (Eur J Surg 1996, 162:823-5)
9. Shuhaiber H. et al. In vitro adherence of bacteria to sutures in cardiac surgery (J Cardiovasc Surg 1989 Sep-Oct, 30(5):749-53)
10. Merritt K. et al. Tissue colonization from implantable biomaterials with low numbers of bacteria (J Biomed Mater Res 1999 Mar 5, 44(3):261-5)
11. Flesh G. TVT for SU: optimizing outcomes

1 μ = 0.001 mm
1N $\hat{=}$ ca. 0.1 kg